Advanced Ultrasound Imaging 2023

Ultrasound Vector Velocity Imaging

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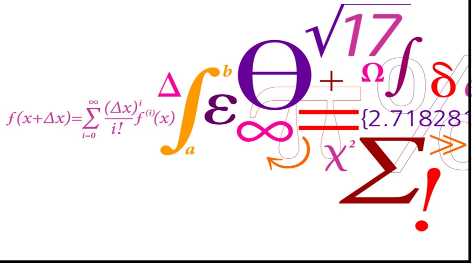

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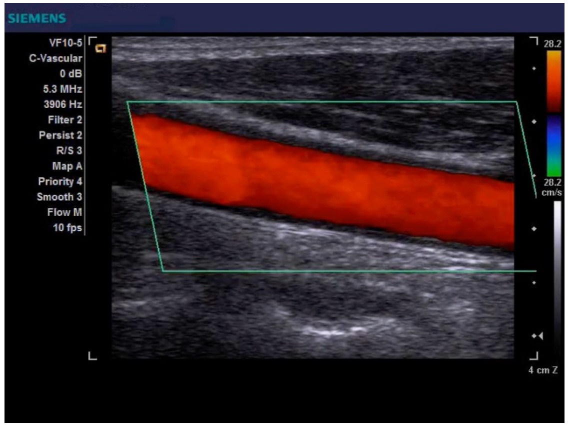
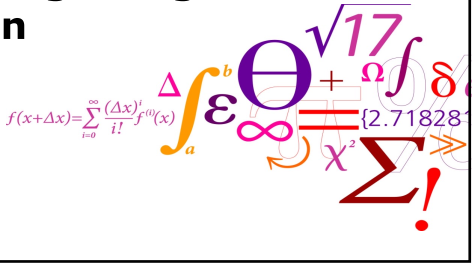
Modern color flow mapping



Ultrasound Vector Velocity Imaging

Part I:

Vector velocity imaging using transverse oscillation



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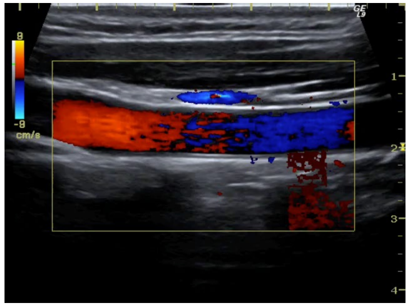
Conventional velocity estimation system

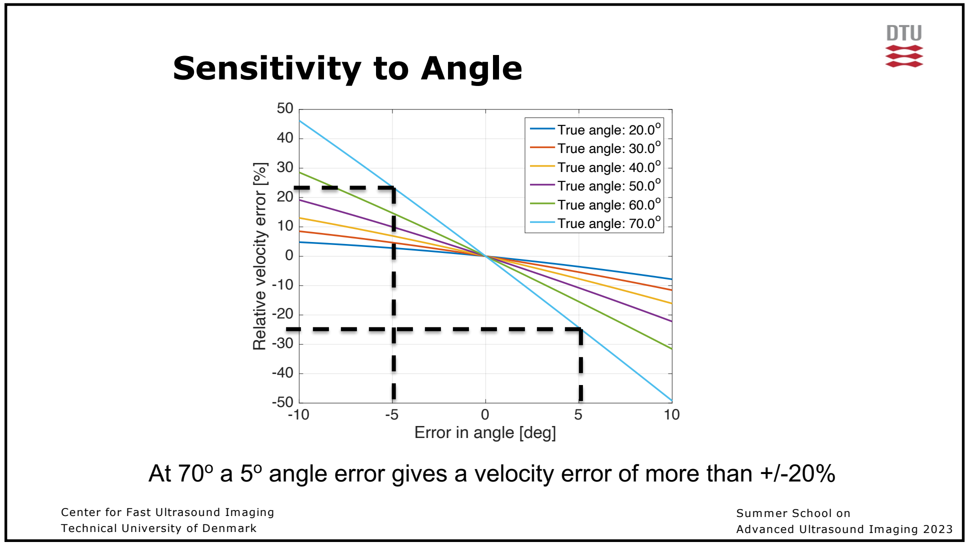
- Low frame rate (approx. 20 Hz)
- Angle dependent velocity estimation



- Velocity changes direction in the image
- Determination is dependent on angle between beam and flow:

$$V_z = |v| \cos(angle)$$

- At 45 degrees:
  71% of velocity
- At 60 degrees:
  50% of velocity
- At 80 degrees:
  17% (!) of velocity
- At 90 degrees
  0%



Sensitivity to Angle

At 70° a 5° angle error gives a velocity error of more than +/-20%

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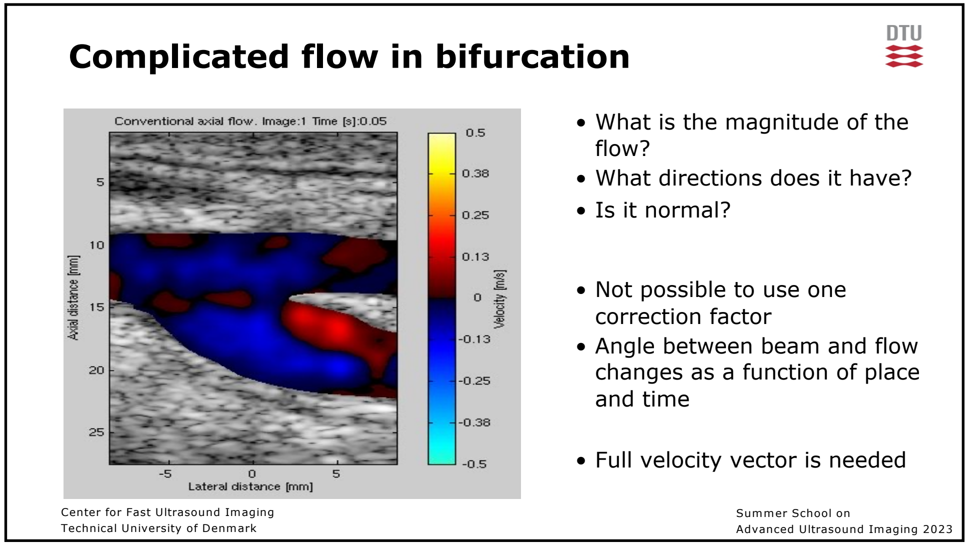

Complicated flow in bifurcation

- What is the magnitude of the flow?
- What directions does it have?
- Is it normal?

- Not possible to use one correction factor
- Angle between beam and flow changes as a function of place and time

- Full velocity vector is needed

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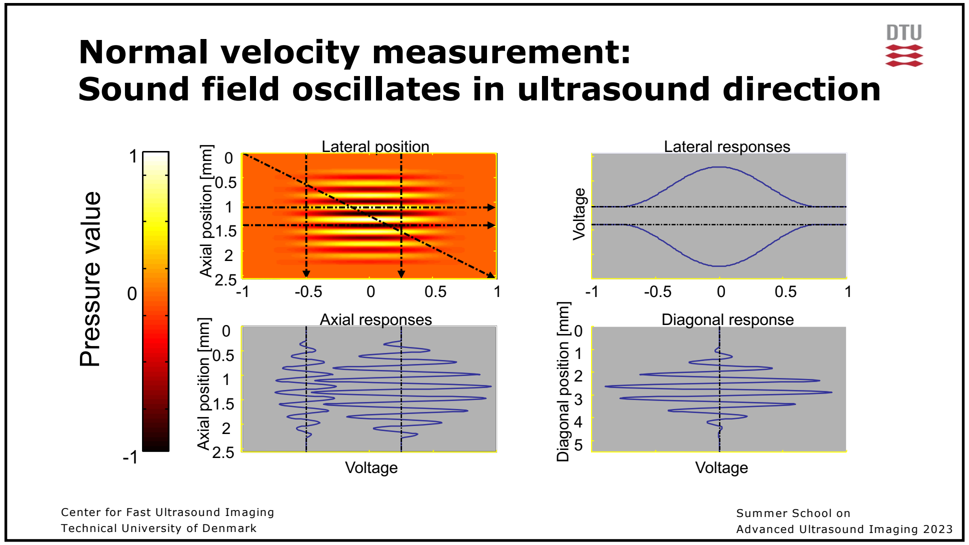

Normal velocity measurement:
Sound field oscillates in ultrasound direction

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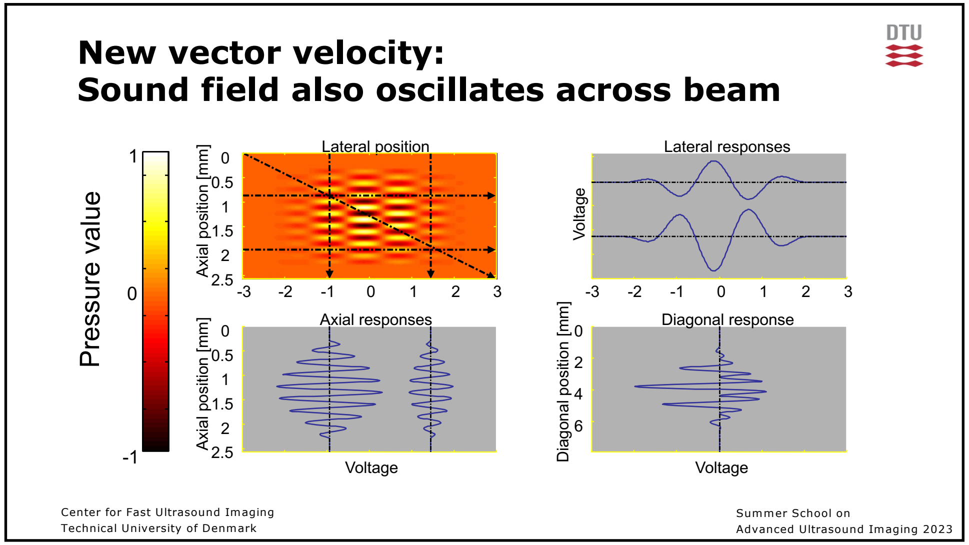

New vector velocity:
Sound field also oscillates across beam

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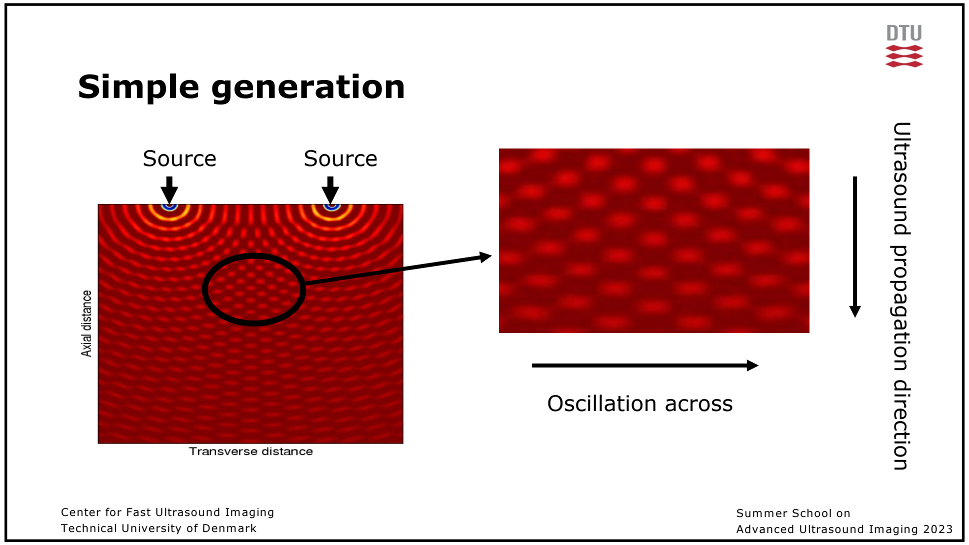
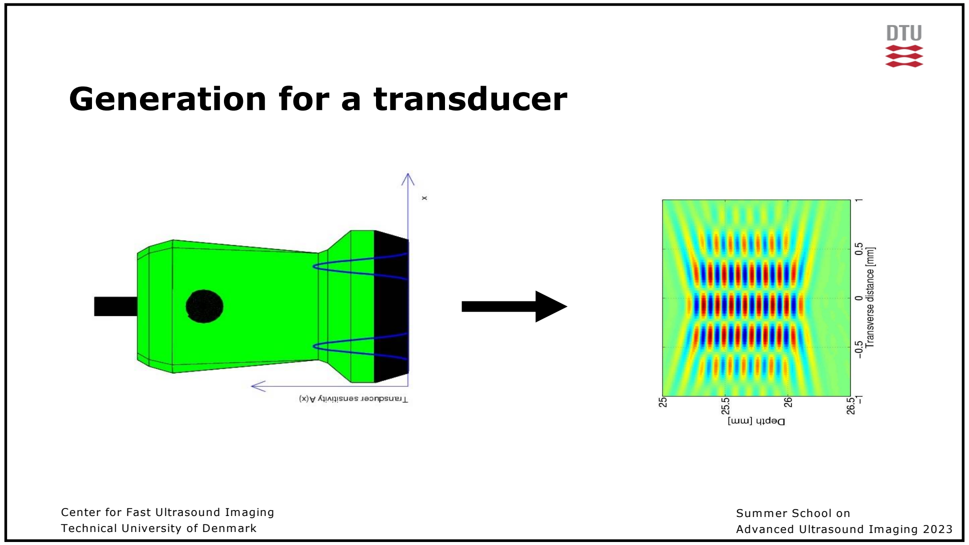
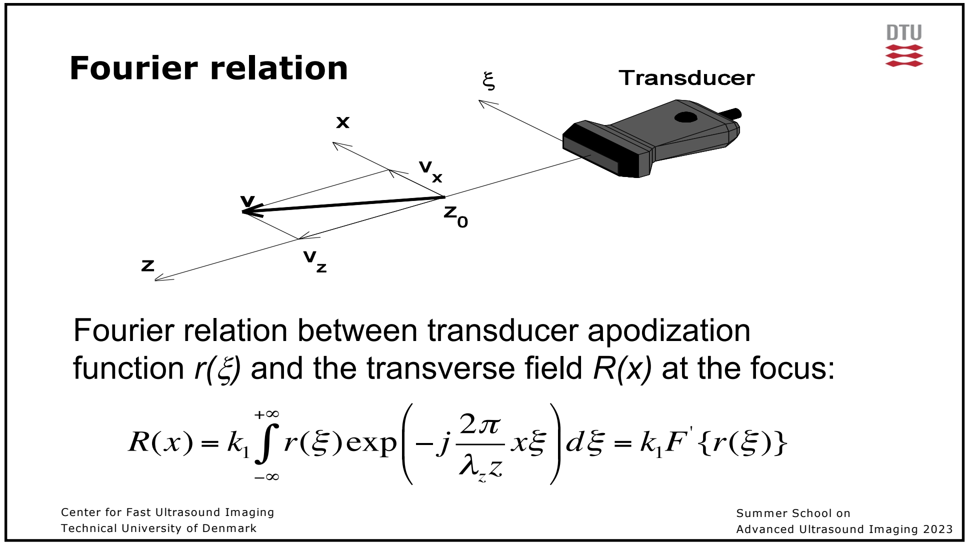


Simple generation



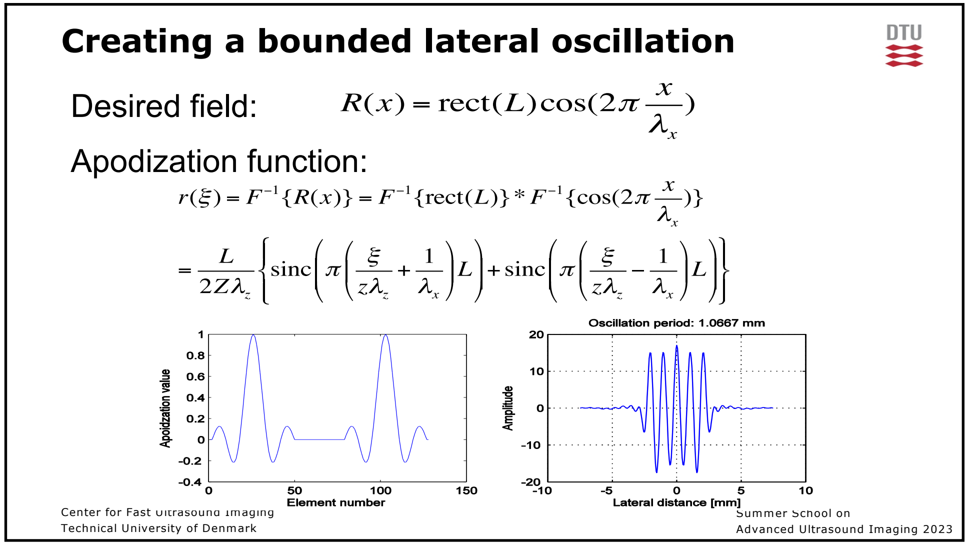
Generation for a transducer



Fourier relation

Fourier relation between transducer apodization function *r(ξ)* and the transverse field *R(x)* at the focus:

$$R(x) = k_1 \int_{-\infty}^{+\infty} r(\xi) \exp\left(-j \frac{2\pi}{\lambda_z z} x\xi\right) d\xi = k_1 F^{'}\{r(\xi)\}$$



Creating a bounded lateral oscillation

Desired field: $R(x) = \text{rect}(L)\cos(2\pi \frac{x}{\lambda_x})$

Apodization function:

$$r(\xi) = F^{-1}\{R(x)\} = F^{-1}\{\text{rect}(L)\} * F^{-1}\{\cos(2\pi \frac{x}{\lambda_x})\}$$

$$= \frac{L}{2Z\lambda_z}\left\{\text{sinc}\left(\pi\left(\frac{\xi}{z\lambda_z} + \frac{1}{\lambda_x}\right)L\right) + \text{sinc}\left(\pi\left(\frac{\xi}{z\lambda_z} - \frac{1}{\lambda_x}\right)L\right)\right\}$$

Lateral oscillation period

- Peak position

$$\frac{\xi_p}{z\lambda_z} = \pm\frac{1}{\lambda_x}$$

- Distance between peaks $2\xi_p = \frac{z\lambda_z}{\lambda_x}$

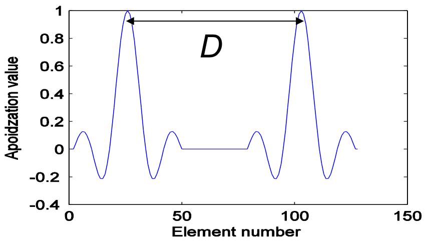
- Lateral oscillation period:

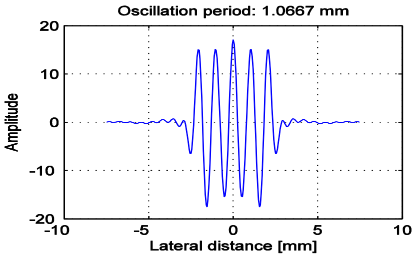
$$\boxed{\lambda_x = \frac{2z\lambda_z}{D}}$$

–*D*: distance between peaks

$$\lambda_x = \frac{2z\lambda_z}{D}$$

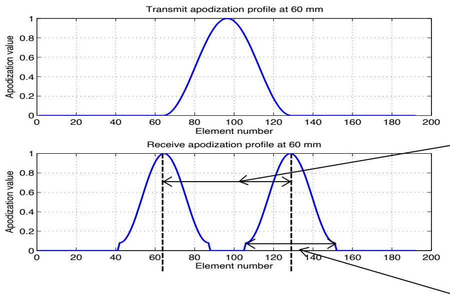
z – depth
D – distance between peaks
λ_z – axial wavelength
λ_x – Lateral oscillation period





Design of Lateral oscillation

$$\lambda_x = \frac{2\lambda z}{D} = \frac{2\lambda z}{N_d P_i}$$



Assume $\lambda_x = 4P_i$.
Distance between peaks:

$$N_d = \frac{2\lambda z}{4P_i^2}$$

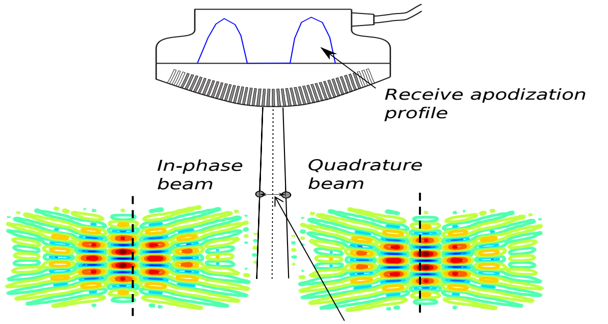
Width of peaks:

$$N_w = \frac{\lambda z}{2F_{\#TO}P_i}$$

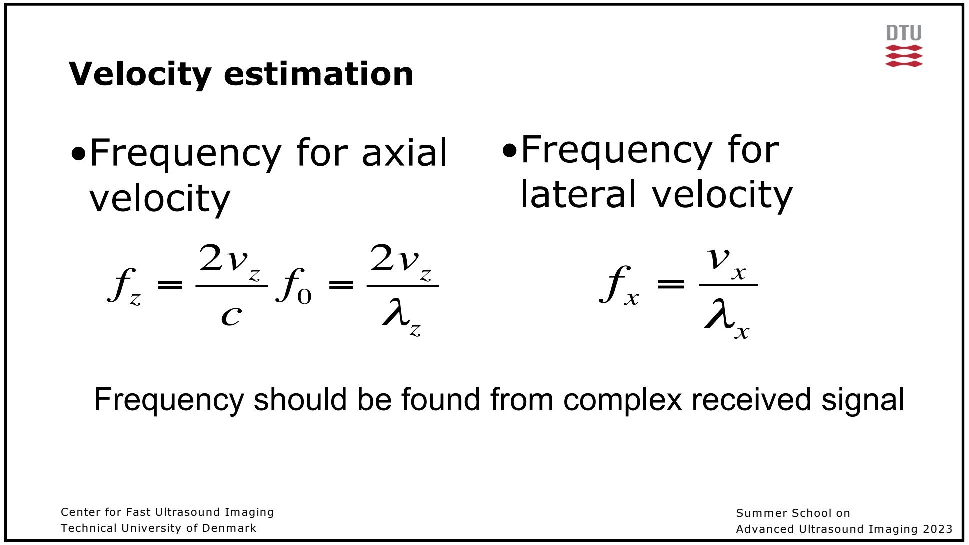
λ – wavelength
D – distance between peaks
$F_{\#TO}$ – F-number for TO

z – depth
P_i – element pitch

In-phase and quadrature fields



Distance between beams is $\lambda_x/4$



Velocity estimation

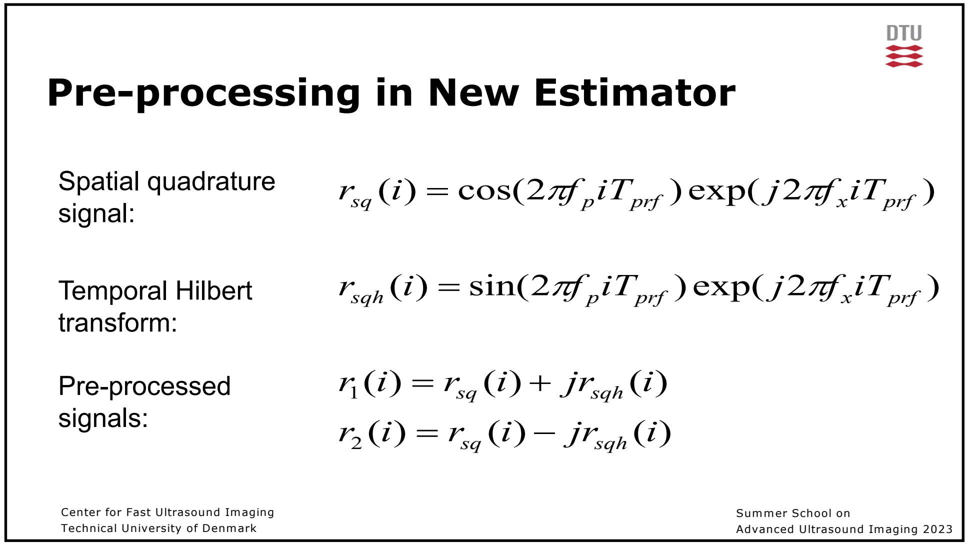
- Frequency for axial velocity

$$f_z = \frac{2v_z}{c} f_0 = \frac{2v_z}{\lambda_z}$$

- Frequency for lateral velocity

$$f_x = \frac{v_x}{\lambda_x}$$

Frequency should be found from complex received signal



Pre-processing in New Estimator

Spatial quadrature signal:

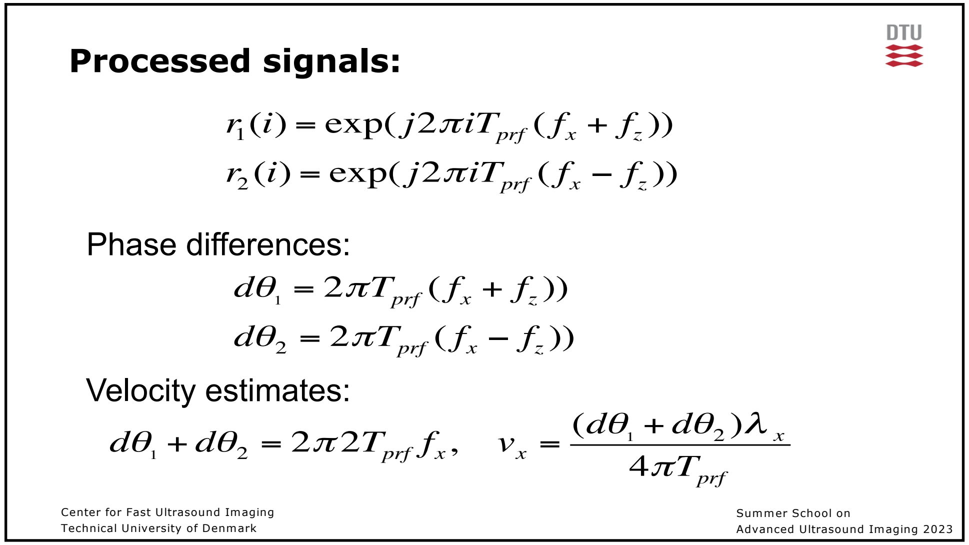
$$r_{sq}(i) = \cos(2\pi f_p i T_{prf}) \exp(j 2\pi f_x i T_{prf})$$

Temporal Hilbert transform:

$$r_{sqh}(i) = \sin(2\pi f_p i T_{prf}) \exp(j 2\pi f_x i T_{prf})$$

Pre-processed signals:

$$r_1(i) = r_{sq}(i) + j r_{sqh}(i)$$
$$r_2(i) = r_{sq}(i) - j r_{sqh}(i)$$



Processed signals:

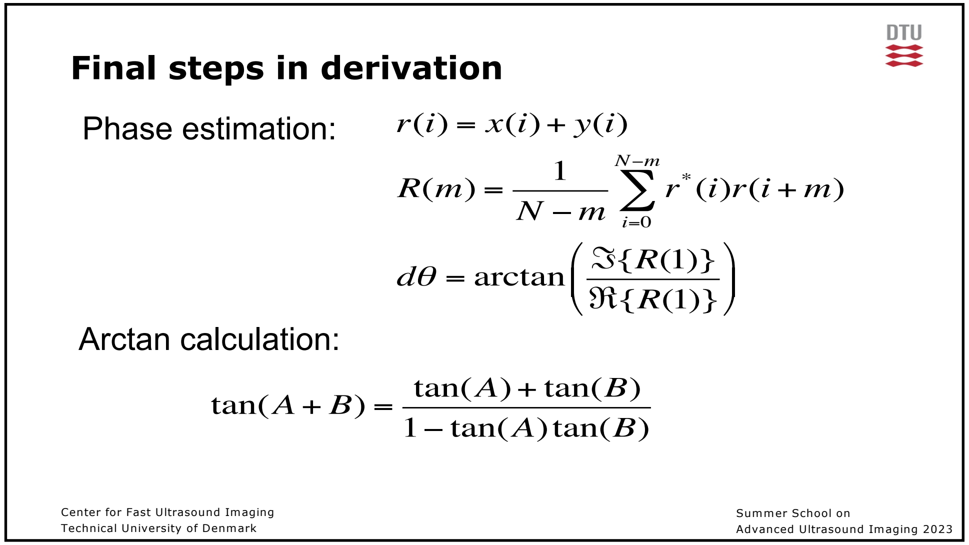
$$r_1(i) = \exp(j 2\pi i T_{prf}(f_x + f_z))$$
$$r_2(i) = \exp(j 2\pi i T_{prf}(f_x - f_z))$$

Phase differences:

$$d\theta_1 = 2\pi T_{prf}(f_x + f_z))$$
$$d\theta_2 = 2\pi T_{prf}(f_x - f_z))$$

Velocity estimates:

$$d\theta_1 + d\theta_2 = 2\pi 2 T_{prf} f_x, \quad v_x = \frac{(d\theta_1 + d\theta_2)\lambda_x}{4\pi T_{prf}}$$



Final steps in derivation

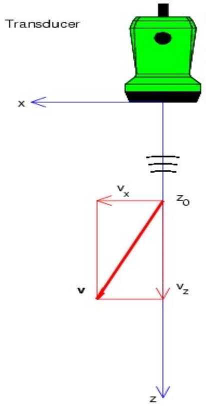
Phase estimation:

$$r(i) = x(i) + y(i)$$
$$R(m) = \frac{1}{N-m} \sum_{i=0}^{N-m} r^*(i) r(i+m)$$
$$d\theta = \arctan\left(\frac{\Im\{R(1)\}}{\Re\{R(1)\}}\right)$$

Arctan calculation:

$$\tan(A+B) = \frac{\tan(A) + \tan(B)}{1 - \tan(A)\tan(B)}$$

Estimation of Velocity



Lateral velocity estimator:

$$v_x = \frac{d_x}{2\pi 2T_{prf}} \arctan\left(\frac{\sum_{i=1}^{N-1} \Im\{R_1(1)\}\Re\{R_2(1)\} + \Im\{R_2(1)\}\Re\{R_1(1)\}}{\sum_{i=1}^{N-1} \Re\{R_1(1)\}\Re\{R_2(1)\} - \Im\{R_1(1)\}\Im\{R_2(1)\}} \right)$$

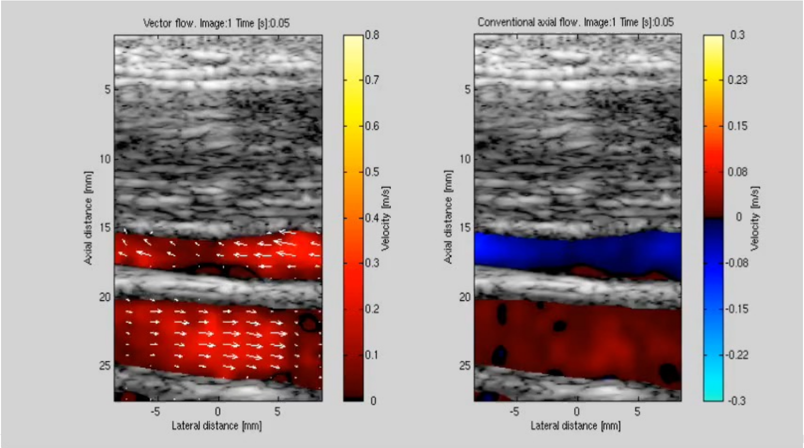
Axial velocity estimator:

$$v_z = \frac{c}{2\pi f_0 4T_{prf}} \arctan\left(\frac{\sum_{i=1}^{N-1} \Im\{R_1(1)\}\Re\{R_2(1)\} - \Im\{R_2(1)\}\Re\{R_1(1)\}}{\sum_{i=1}^{N-1} \Re\{R_1(1)\}\Re\{R_2(1)\} + \Im\{R_1(1)\}\Im\{R_2(1)\}} \right)$$

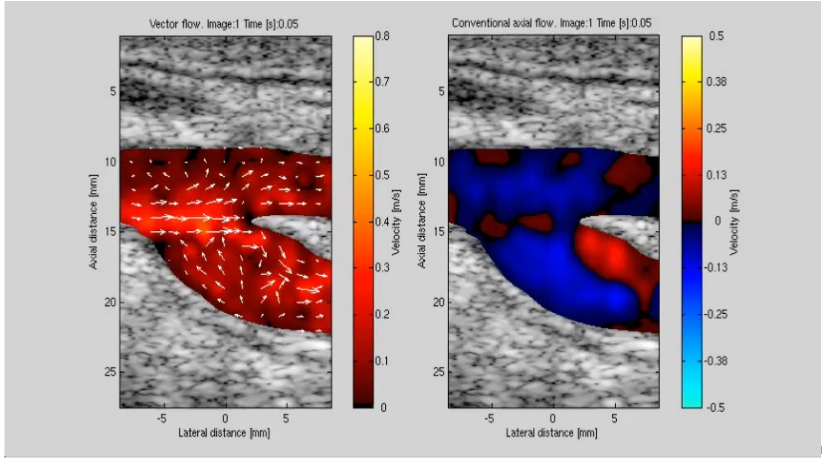
RASMUS

- Remotely Accessible Software programmable Multi-channel Ultrasound System
- Can be used for synthetic aperture, real-time, *in-vivo* data acquisition
- Made solely for research purposes

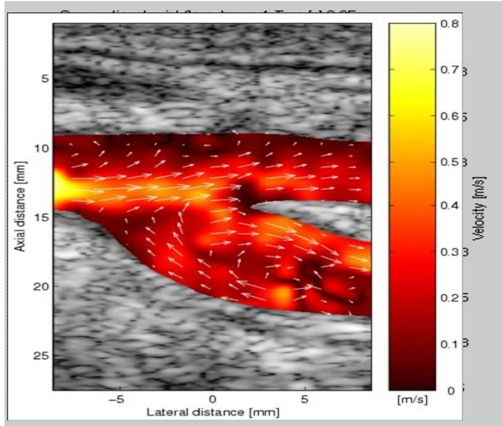
In-vivo vector velocity for carotid artery and jugular vein



Velocity in carotid bifurcation



Complicated flow in bifurcation



New Transverse Estimator

$$v_x = \frac{\lambda_x}{2\pi 2T_{prf}} \arctan\left(\frac{\Im\{R_1(1)\}\Re\{R_2(1)\} + \Im\{R_2(1)\}\Re\{R_1(1)\}}{\Re\{R_1(1)\}\Re\{R_2(1)\} - \Im\{R_1(1)\}\Im\{R_2(1)\}}\right)$$

$$v_z = \frac{\lambda}{2\pi 4T_{prf}} \arctan\left(\frac{\Im\{R_1(1)\}\Re\{R_2(1)\} - \Im\{R_2(1)\}\Re\{R_1(1)\}}{\Re\{R_1(1)\}\Re\{R_2(1)\} + \Im\{R_1(1)\}\Im\{R_2(1)\}}\right)$$

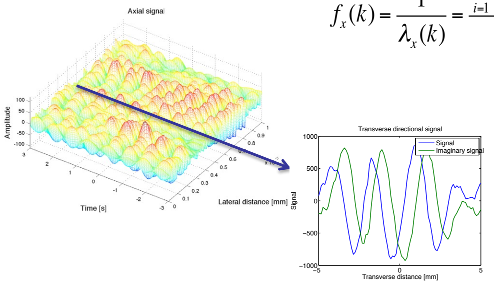
$$R_1(l) = \frac{1}{(N-1)N_d N_s} \sum_{i=1}^{N-1} \sum_{n=1}^{N_d} \sum_{k=-N_s/2}^{N_s/2} r_1^*(k+N_z,n,i)\, r_1(k+N_z,n,i+l)$$

$$R_2(l) = \frac{1}{(N-1)N_d N_s} \sum_{i=1}^{N-1} \sum_{n=1}^{N_d} \sum_{k=-N_s/2}^{N_s/2} r_2^*(k+N_z,n,i)\, r_2(k+N_z,n,i+l)$$

R_1 - Complex autocorrelation of signal one averaged over directional signal and depth
R_2 - Complex autocorrelation of signal two
N_z – RF sample depth for velocity estimate

Calculation of Mean Lateral Oscillation Wavelength

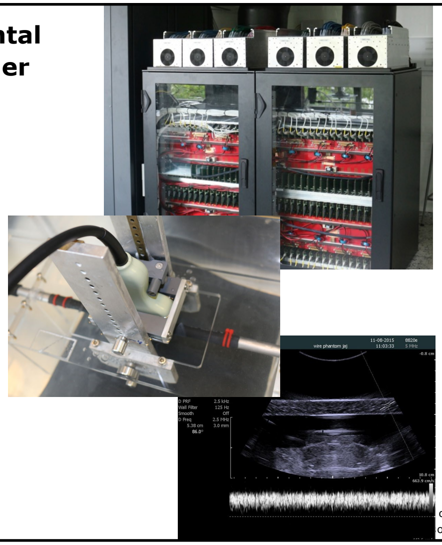
$$f_x(k) = \frac{1}{\lambda_x(k)} = \frac{\sum_{i=1}^{N_c} \sum_{m=-N/2}^{N/2} \frac{m}{N\Delta x} R_{sq}(k,m,i)}{\sum_{i=1}^{N_c} \sum_{m=-N/2}^{N/2} R_{sq}(k,m,i)}$$



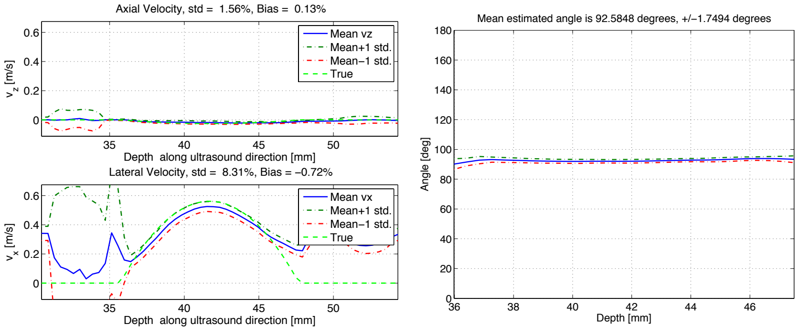
$R_{sq}(k,m,i)$ – Fourier transform of lateral signal at sample *k* and emission *i*

SARUS Experimental Ultrasound Scanner

- 192 channels sampled at 17.5 MHz/12 bits
- 129 B-mode emissions
- Interspaced with VFI emissions focused at 105 mm
- f_{prf}=5 kHz
- BK Medical 8820e 3 MHz convex array probe used
- Data acquired for 30 frames
- Acquired on rig with parabolic flow



Velocity Profiles at 40 mm using 16 Emissions at 90° Beam-to-flow Angle

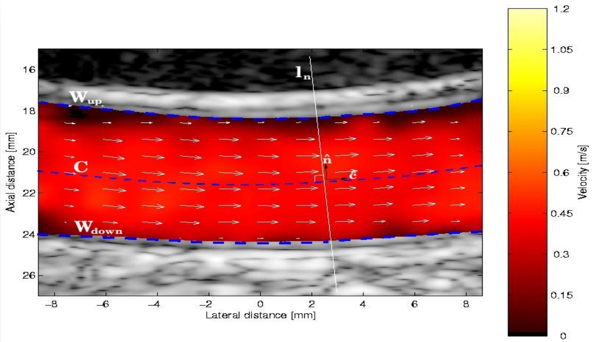


V_x std: 8.31%, bias -0.72%, angle std: 1.75 degrees

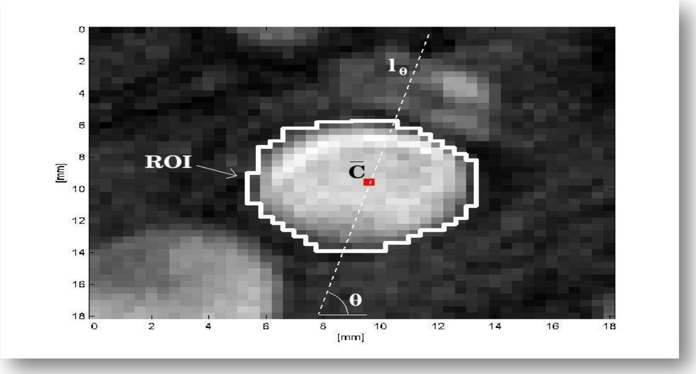
Is it Accurate? Clinical study

- 11 healthy volunteers
  - seven males and four females,
  - 24 – 44 years old, mean age: 32 years)
- Each person was scanned by US and MRI
  - Examination for every person were performed at two separate occasions with no more than a week in between.
  - The volunteer rested supine 15 minutes prior to both examinations.
  - All scans were carried out by an experienced radiologist.

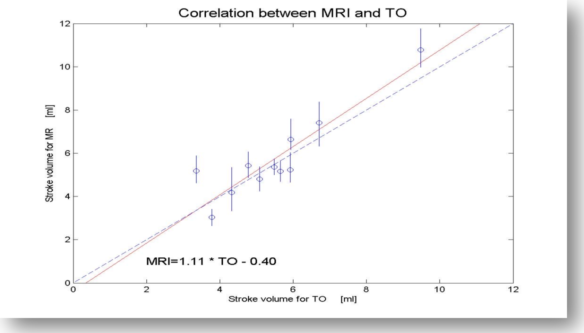
Vector Velocity Image of Stroke Volume



MR Measurement of Volume Flow



Clinical Validation of Vector Flow against MR



R = 0.91, P<0.01

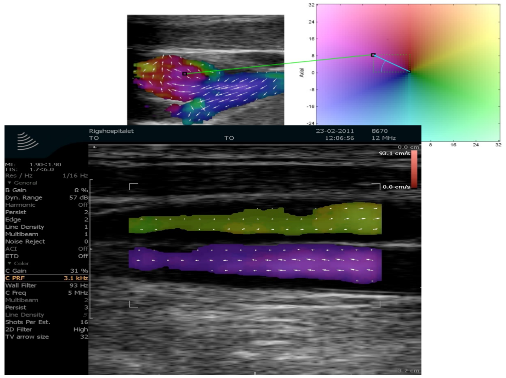
95% CI for R: 0.69 to 0.98

Regression line:

MRI = 1.1 * TO – 0.4 ml

Vertical bars indicate range for rotational symmetry assumption.

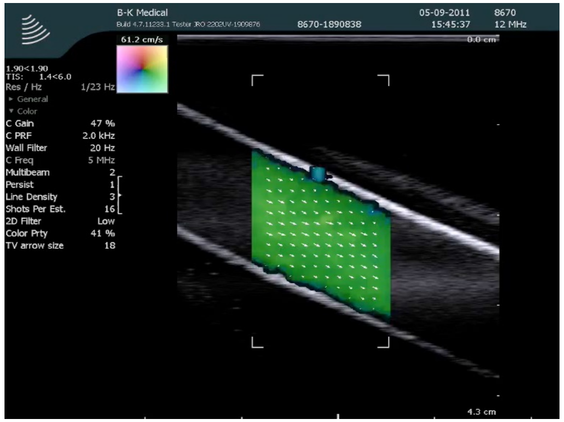
Commercial implementation: BK Medical ProFocus scanner FDA approved January, 2012



Rigshospitalet
TO
TO
23-02-2011
12:06:56
8670
12 MHz

MI: 1.90<1.90
TIS: 1.7<6.0
Res / Hz 1/16 Hz
▼ General
B Gain 8 %
Dyn. Range 57 dB
Harmonic Off
Persist 2
Edge 2
Line Density 1
Multibeam 1
Noise Reject 0
ACI Off
ETD Off
▼ Color
C Gain 31 %
C PRF 3.1 kHz
Wall Filter 93 Hz
C Freq 5 MHz
Multibeam 2
Persist 3
Line Density 5
Shots Per Est. 16
2D Filter High
TV arrow size 32

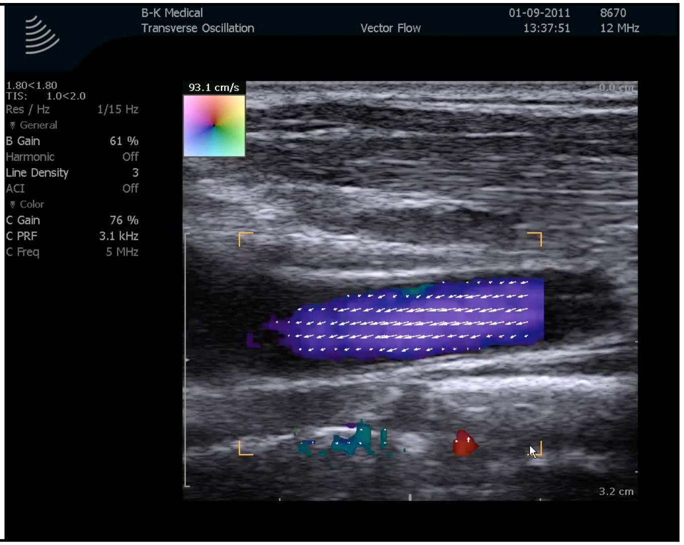
Display of velocity



B-K Medical
Build 4.7.11233.1 Tester JRO 2202UV-1909876
8670-1890838
05-09-2011
15:45:37
8670
12 MHz

1.90<1.90
TIS: 1.4<6.0
Res / Hz 1/23 Hz
▸ General
▼ Color
C Gain 47 %
C PRF 2.0 kHz
Wall Filter 20 Hz
C Freq 5 MHz
Multibeam 2
Persist 1
Line Density 3
Shots Per Est. 16
2D Filter Low
Color Prty 41 %
TV arrow size 18

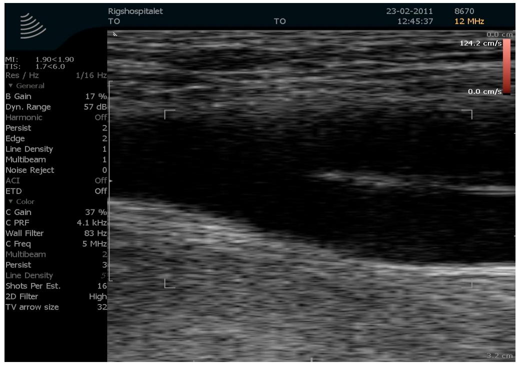
Scanning of the carotid artery



B-K Medical
Transverse Oscillation
Vector Flow
01-09-2011
13:37:51
8670
12 MHz

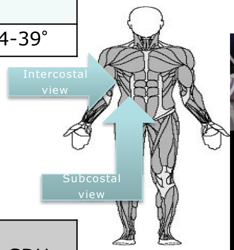
1.80<1.80
TIS: 1.0<2.0
Res / Hz 1/15 Hz
▼ General
B Gain 61 %
Harmonic Off
Line Density 3
ACI Off
▼ Color
C Gain 76 %
C PRF 3.1 kHz
C Freq 5 MHz

Bifurcation in Femoral Artery

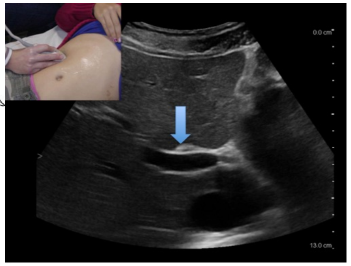


Influence of Beam-to-flow Angle

TO	SDU
10-61°	4-39°

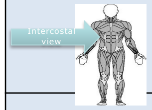
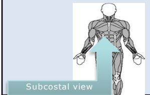


TO	SDU
53-130°	57-99°

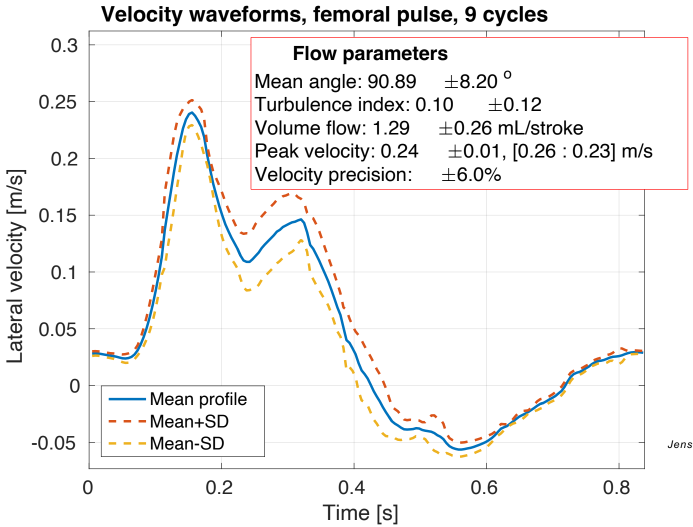


From Brandt et al., IEEE IUS, 2015

Estimated Peak Velocities

	Mean TO (SD)	Mean SDU (SD)	*P*-value
 Intercostal view	0.203±(0.038) m/s	0.202±(0.029) m/s	0.94
 Subcostal view	0.180±(0.034) m/s	0.320±(0.060) m/s	0.001
P-value	0.26	0.001	

From Brandt et al., IEEE IUS, 2015

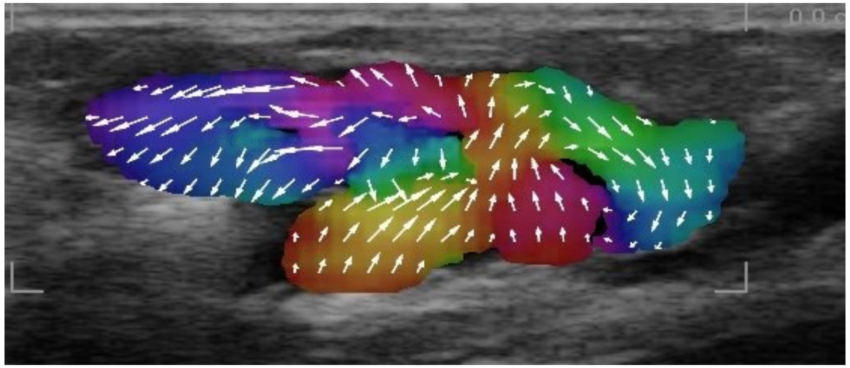


Flow parameters

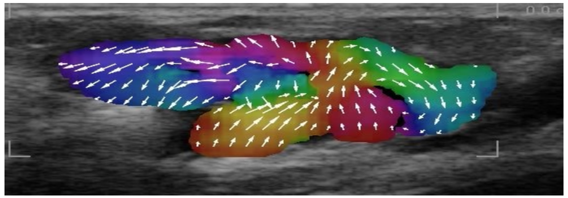
Mean angle: 90.89 ±8.20 °
Turbulence index: 0.10 ±0.12
Volume flow: 1.29 ±0.26 mL/stroke
Peak velocity: 0.24 ±0.01, [0.26 : 0.23] m/s
Velocity precision: ±6.0%

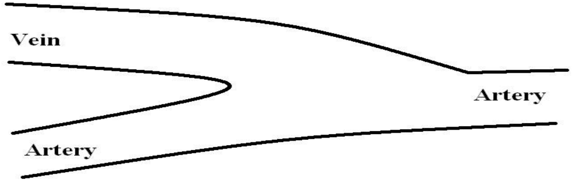
Jensen, IEEE UFFC, 2017, 64(8), pp. 1194-1204

Vein-artery connection for kidney hemodialysis patient

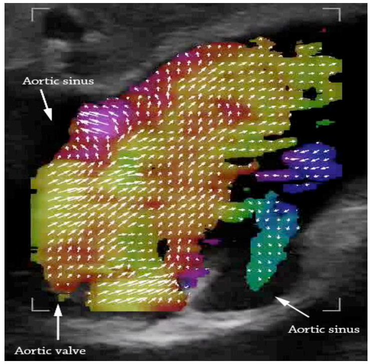


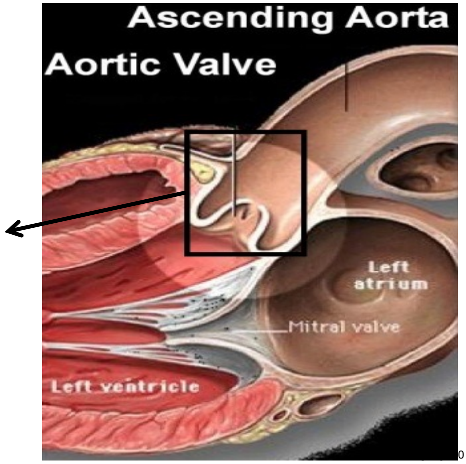
Anatomy of vein-artery graft



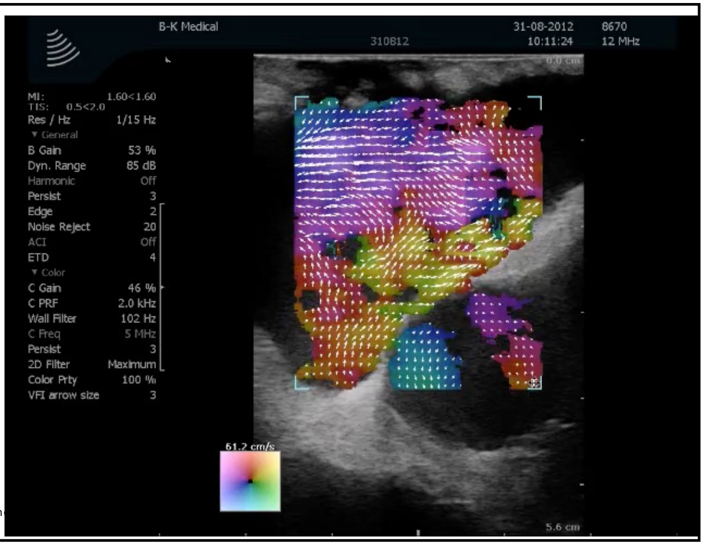


Anatomy of Intercardiac Scan of Right Atrium





Intercardiac scan Right Atrium



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B-K Medical                          31-08-2012   8670
                      310812           10:11:24   12 MHz
MI:             1.60<1.60
TIS:    0.5<2.0
Res / Hz          1/15 Hz
 ▼ General
B Gain               53 %
Dyn. Range          85 dB
Harmonic              Off
Persist                 3
Edge                    2
Noise Reject           20
ACI                   Off
ETD                     4
 ▼ Color
C Gain               46 %
C PRF             2.0 kHz
Wall Filter        102 Hz
C Freq              5 MHz
Persist                 3
2D Filter         Maximum
Color Prty          100 %
VFI arrow size          3
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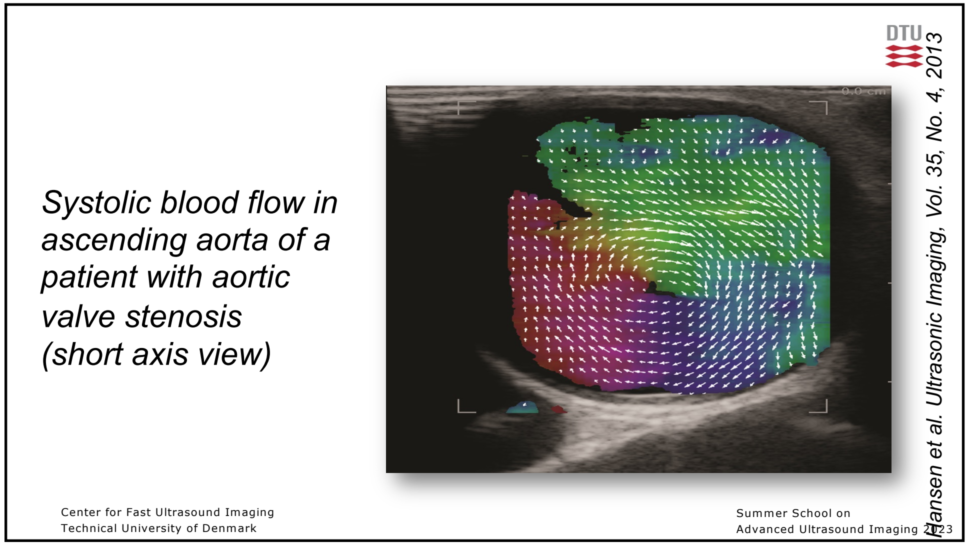
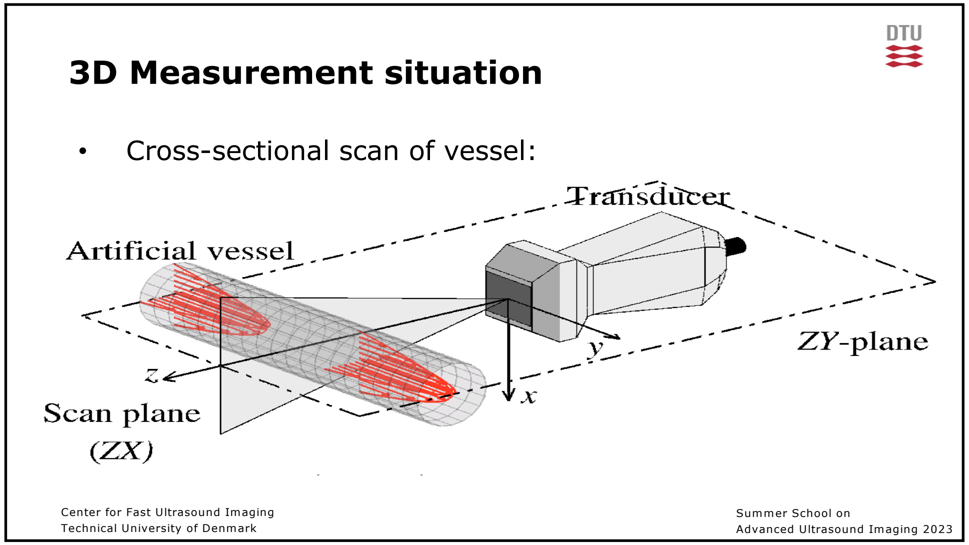


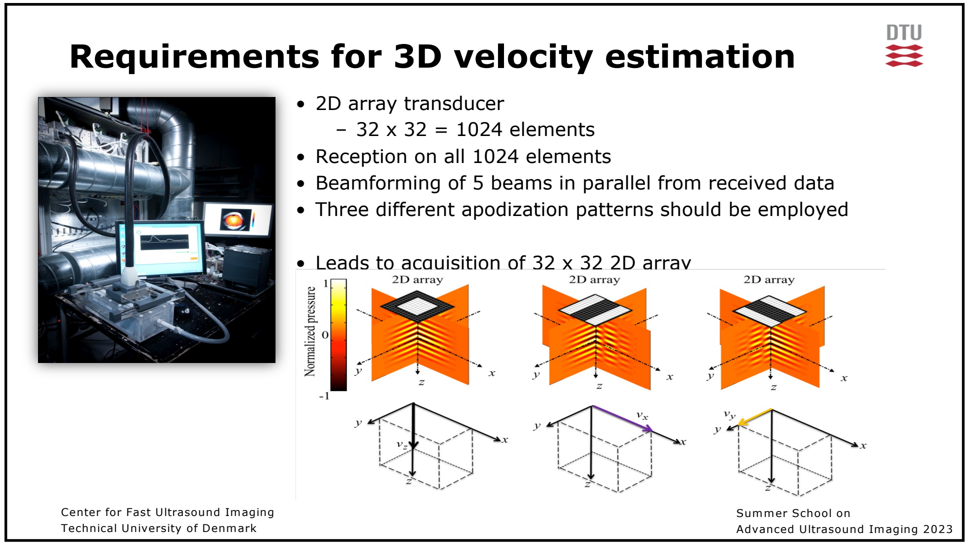
Systolic blood flow in ascending aorta of a patient with aortic valve stenosis (short axis view)

Hansen et al. Ultrasonic Imaging, Vol. 35, No. 4, 2013



3D Measurement situation

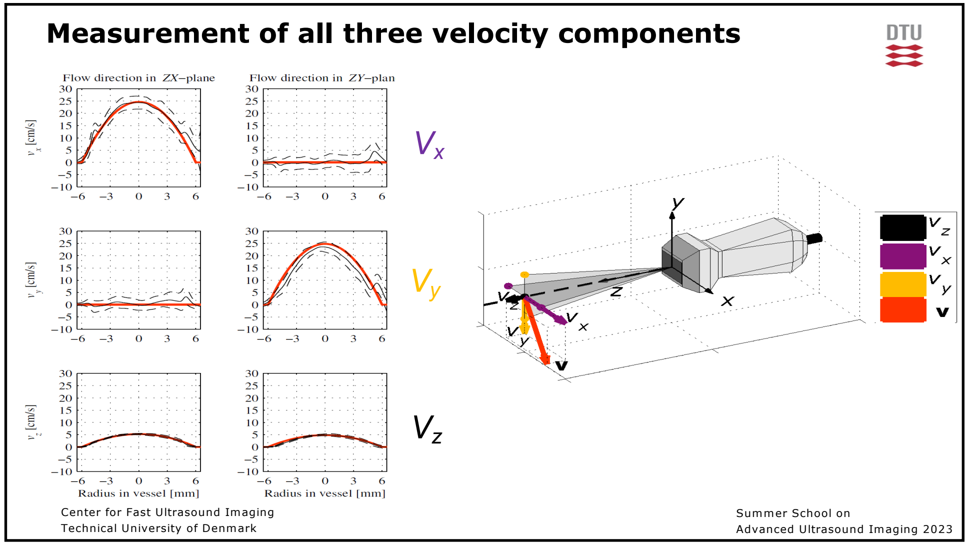
- Cross-sectional scan of vessel:



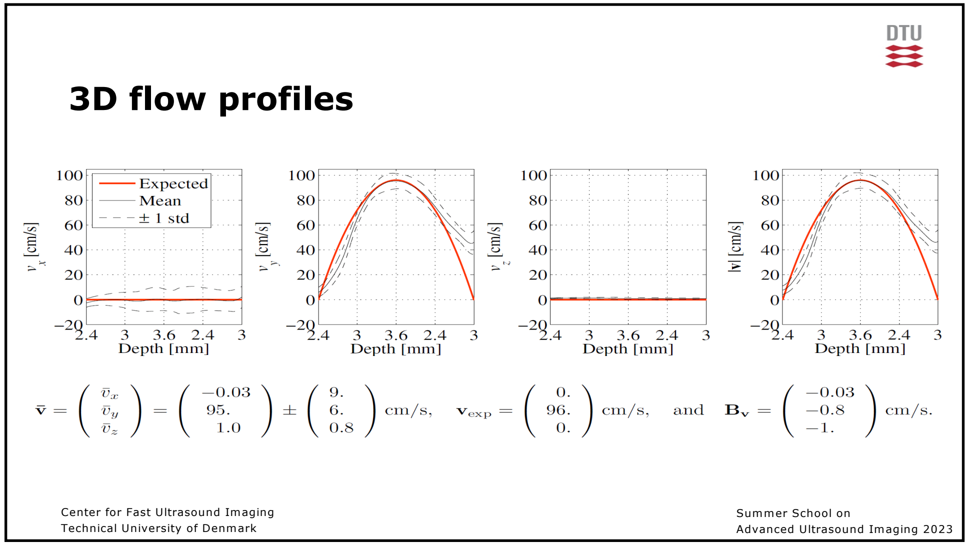
Requirements for 3D velocity estimation

- 2D array transducer
  - 32 x 32 = 1024 elements
- Reception on all 1024 elements
- Beamforming of 5 beams in parallel from received data
- Three different apodization patterns should be employed

- Leads to acquisition of 32 x 32 2D array



Measurement of all three velocity components



3D flow profiles

$$\bar{\mathbf{v}} = \begin{pmatrix} \bar{v}_x \\ \bar{v}_y \\ \bar{v}_z \end{pmatrix} = \begin{pmatrix} -0.03 \\ 95. \\ 1.0 \end{pmatrix} \pm \begin{pmatrix} 9. \\ 6. \\ 0.8 \end{pmatrix} \text{cm/s}, \quad \mathbf{v}_{\text{exp}} = \begin{pmatrix} 0. \\ 96. \\ 0. \end{pmatrix} \text{cm/s}, \quad \text{and} \quad \mathbf{B_v} = \begin{pmatrix} -0.03 \\ -0.8 \\ -1. \end{pmatrix} \text{cm/s}.$$

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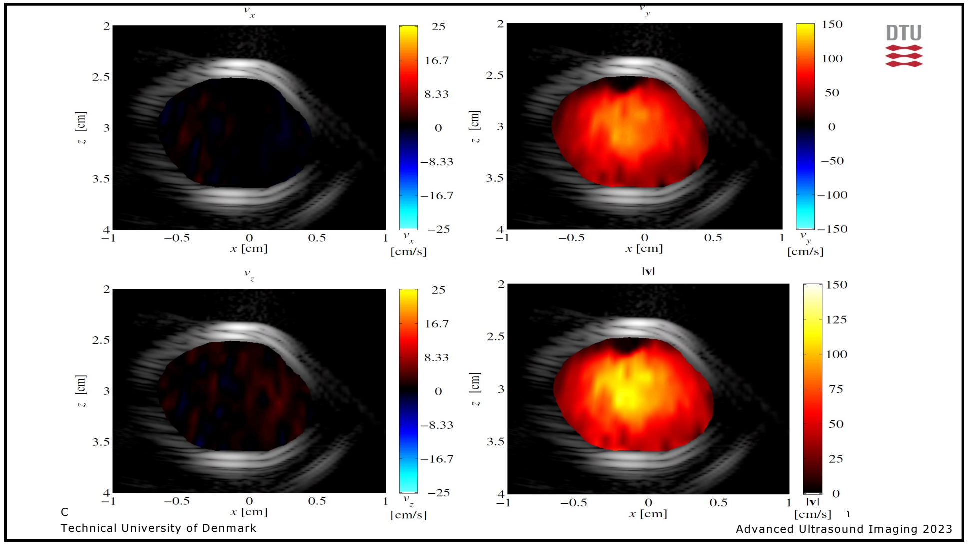
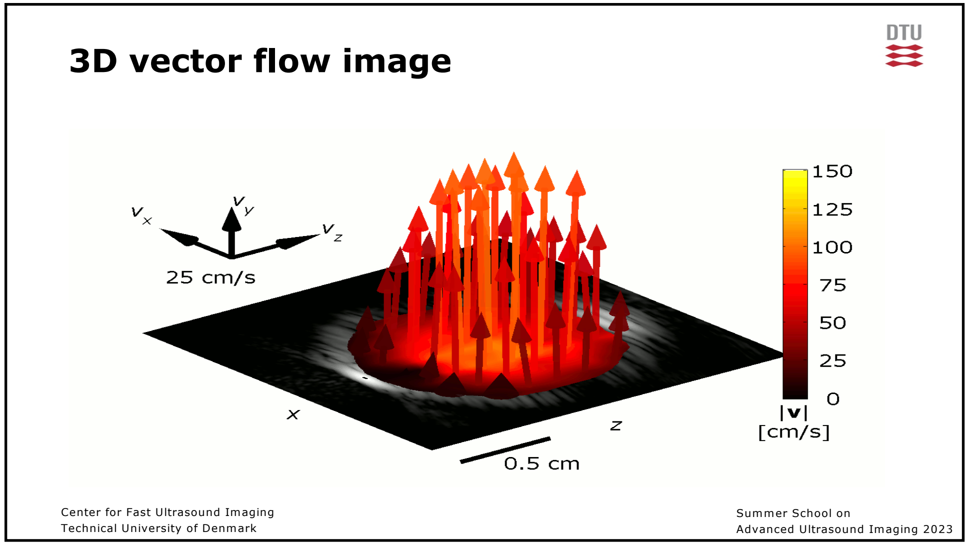


50



3D vector flow image

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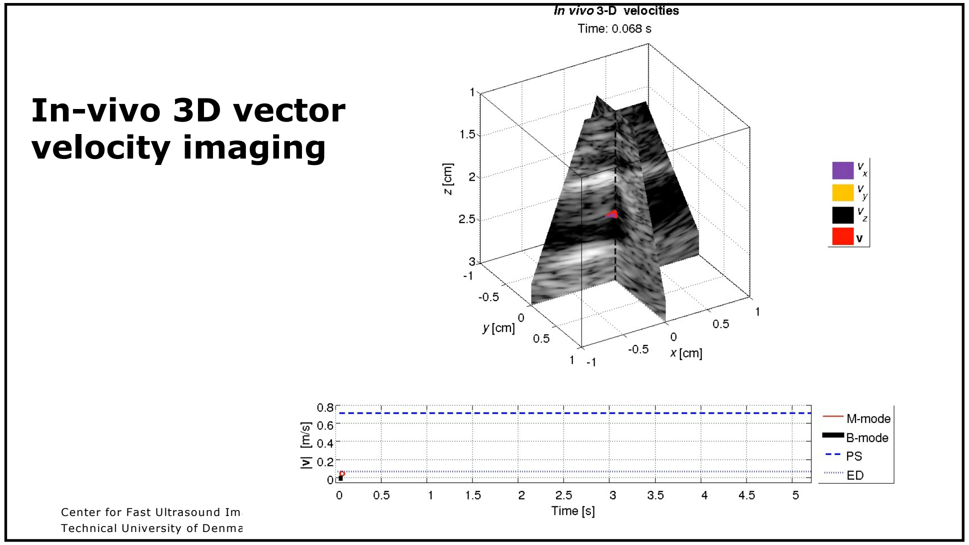

In-vivo 3D vector velocity imaging

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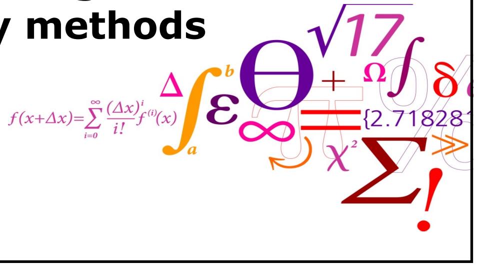
Ultrasound Vector Velocity Imaging

Part II:

Directional beamforming and other vector velocity methods

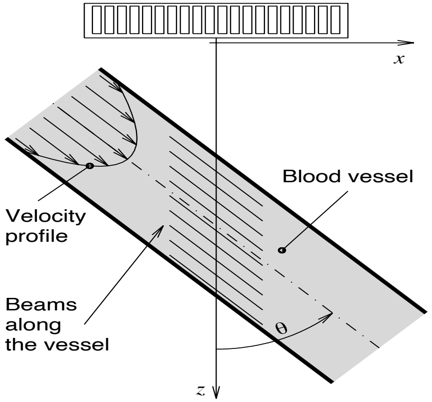


Center for Fast Ultrasound Imaging
Department of Health Technology

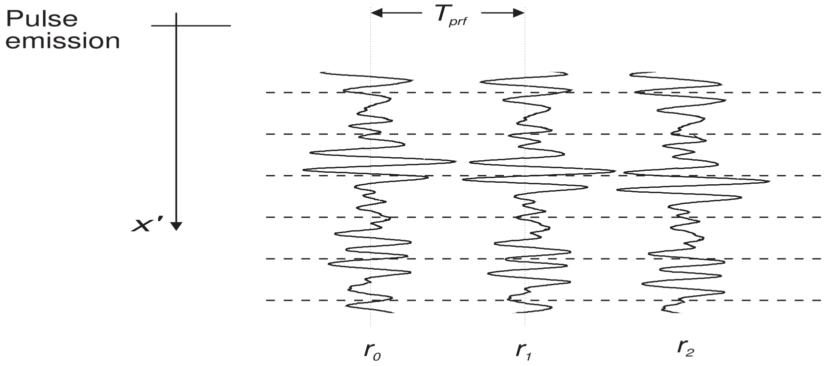
Outline

- Directional beamforming
  - –Beamformation
  - –Angle estimation
- Crossed beams velocity estimation
- Speckle tracking
- Finding the angle from the spectral display

Directional beamforming



Cross-correlation of directional lines



Cross-Correlation to Find Velocity

$$R_{12}(n) = \frac{1}{M}\sum_{j=0}^{M-1} r_1(j)r_2(j+n)$$

$$= \frac{1}{M}\sum_{j=0}^{M-1} r_1(j)r_1(j+n-n_s)$$

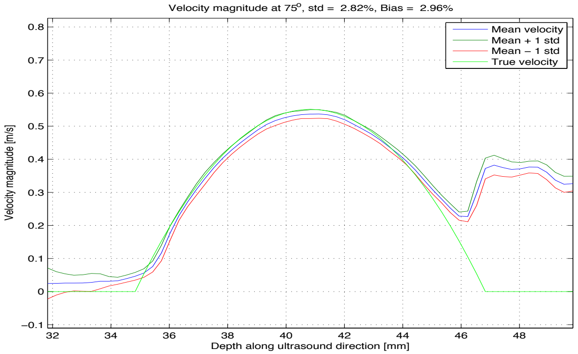
$$R_{12}(n) = R_{11}(n-n_s)$$

Velocity estimate is:

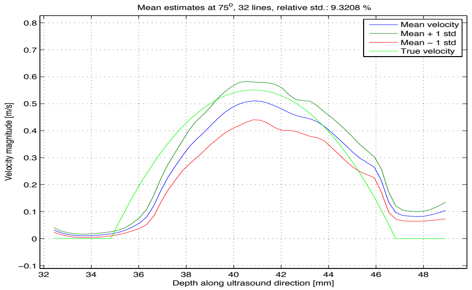
$$v_{mag} = \frac{n_s \Delta x'}{T_{prf}}$$

Velocity profiles for directional beamforming

75° flow angle, 16 emissions/estimate, line length: 20 λ

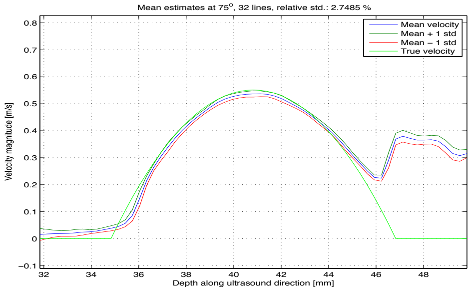


Performance using the same data



Transverse oscillation

9.3%



Directional beamforming

2.7%

Number of calculations

Transverse oscillation

$$N_{TO} = (4 \cdot 28 N_s)\frac{f_s}{N_s}F_f$$

Directional beamforming

$$N_d = (N_l^2 + N_l)\frac{f_s}{N_s}F_f$$

Ratio:

$$R_c = \frac{N_d}{N_{TO}} = \frac{(N_l^2 + N_l)}{4 \cdot 28 N_s}$$

Typical values: N_l =100, N_s = 8 gives ***R_c = 11.3***

Neglects finding the velocity direction

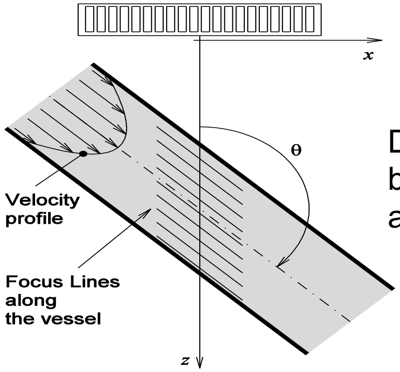
N_l – Number samples in directional line

f_s – Sampling frequency

N_s – Number of RF samples in estimate

F_f – Fraction of time for flow

Determination at Different Angles



Directional lines are beamformed at different angles

Determination of Velocity Angle

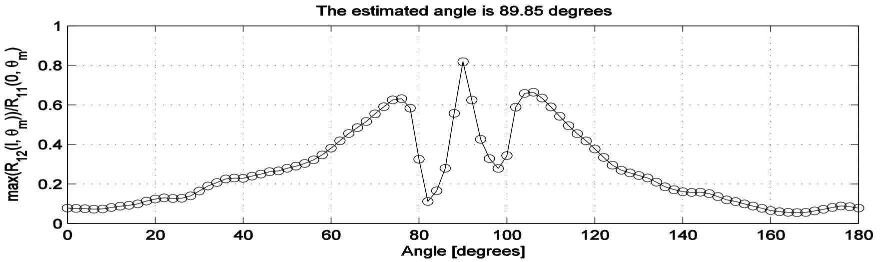
$$R_{12n}(\theta) = \frac{\max\{R_{12}(k,\theta)\}}{R_{12}(0,\theta)}$$

$$\theta_m = ArgMax(R_{12n}(\theta))$$

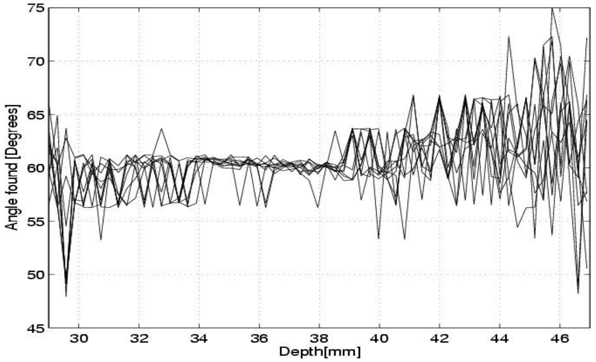
Angle is found from maximum in normalized peak value of cross-correlation function.

Value is interpolated using a second order polynomial to increase the accuracy.

Angle Determination at 90 deg



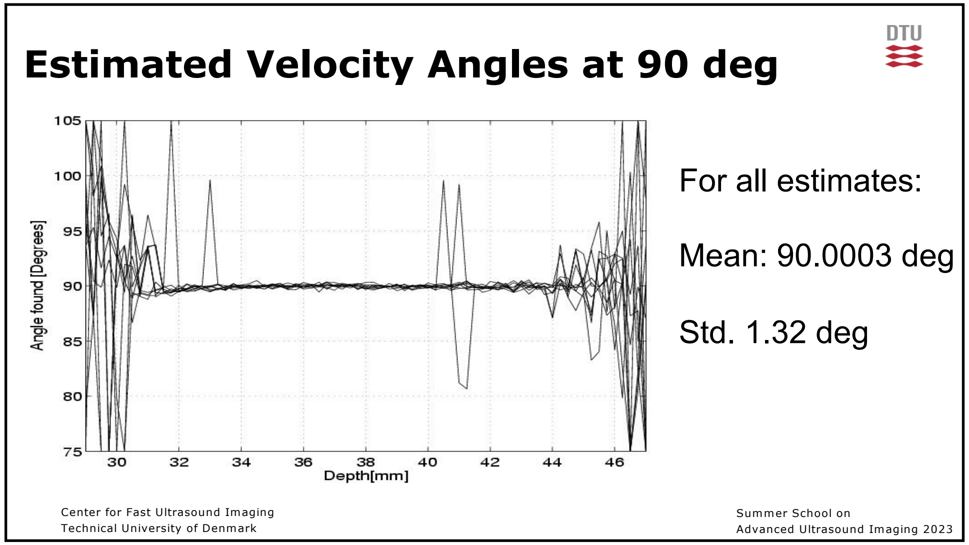
Estimated Velocity Angles at 60 deg



For all estimates:

Mean: 60.54 deg

Std. 2.1 deg

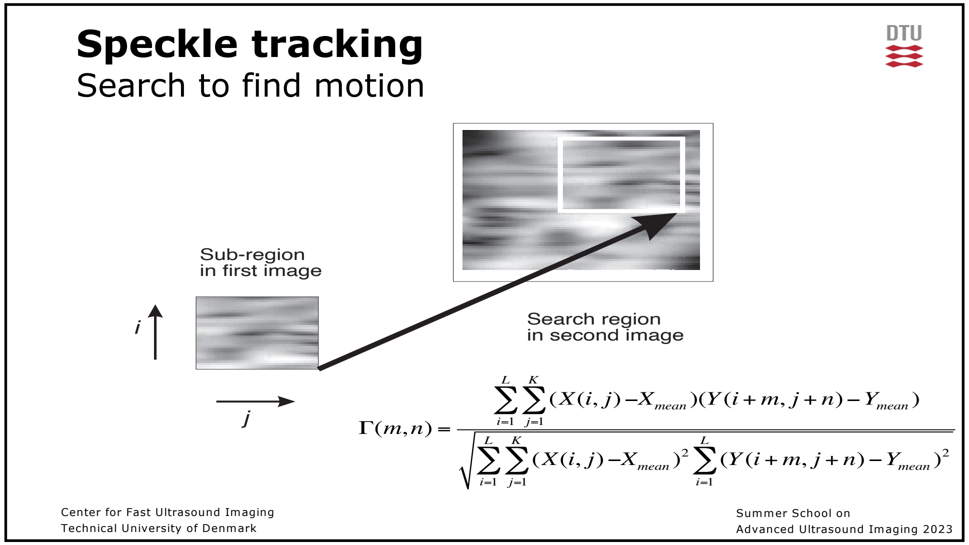


Estimated Velocity Angles at 90 deg

For all estimates:

Mean: 90.0003 deg

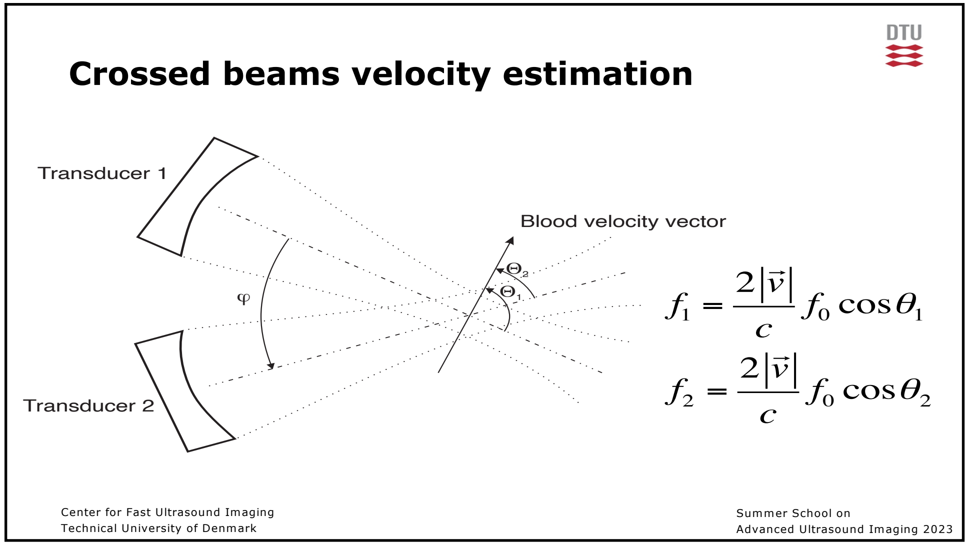
Std. 1.32 deg



Speckle tracking

Search to find motion

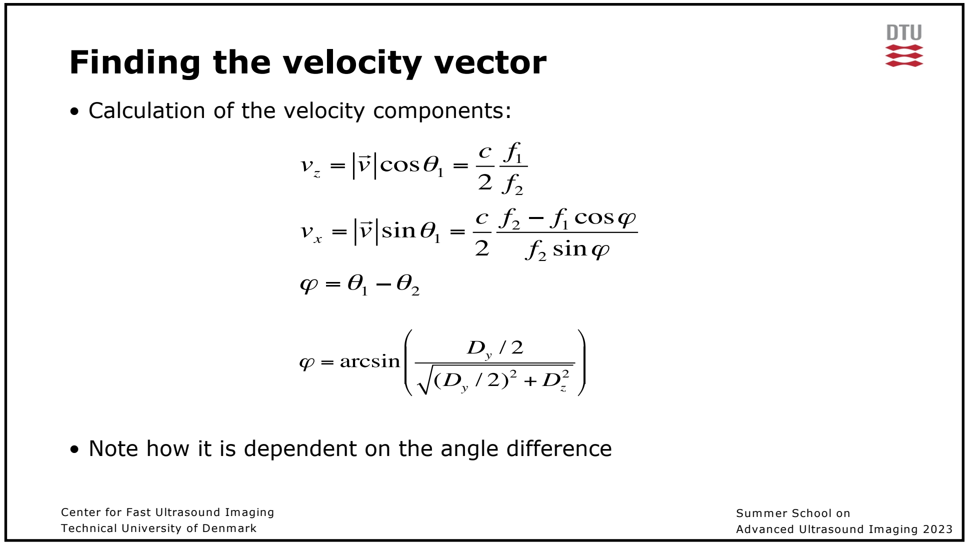
$$\Gamma(m,n)=\frac{\sum_{i=1}^{L}\sum_{j=1}^{K}(X(i,j)-X_{mean})(Y(i+m,j+n)-Y_{mean})}{\sqrt{\sum_{i=1}^{L}\sum_{j=1}^{K}(X(i,j)-X_{mean})^2\sum_{i=1}^{L}(Y(i+m,j+n)-Y_{mean})^2}}$$



Crossed beams velocity estimation

$$f_1=\frac{2|\vec{v}|}{c}f_0\cos\theta_1$$

$$f_2=\frac{2|\vec{v}|}{c}f_0\cos\theta_2$$



Finding the velocity vector

- Calculation of the velocity components:

$$v_z=|\vec{v}|\cos\theta_1=\frac{c}{2}\frac{f_1}{f_2}$$

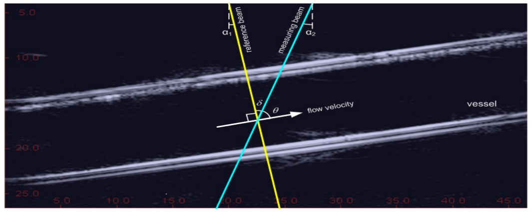
$$v_x=|\vec{v}|\sin\theta_1=\frac{c}{2}\frac{f_2-f_1\cos\varphi}{f_2\sin\varphi}$$

$$\varphi=\theta_1-\theta_2$$

$$\varphi=\arcsin\left(\frac{D_y/2}{\sqrt{(D_y/2)^2+D_z^2}}\right)$$

- Note how it is dependent on the angle difference

Dual beam method



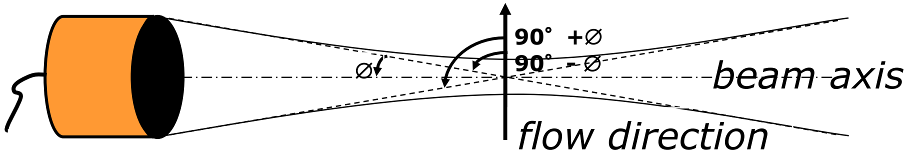
<u>Assumption</u>:

A reference beam can be <u>transversely</u> <u>oriented</u> to the flow direction

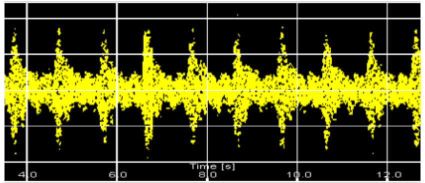
Angle estimation is based on inspection of the (transverse) Doppler spectrum

Slide courtesy of Piero Tortoli, University of Florence

Transverse Doppler spectrum



The flow is interrogated by a range of angles around the nominal 90° Doppler angle

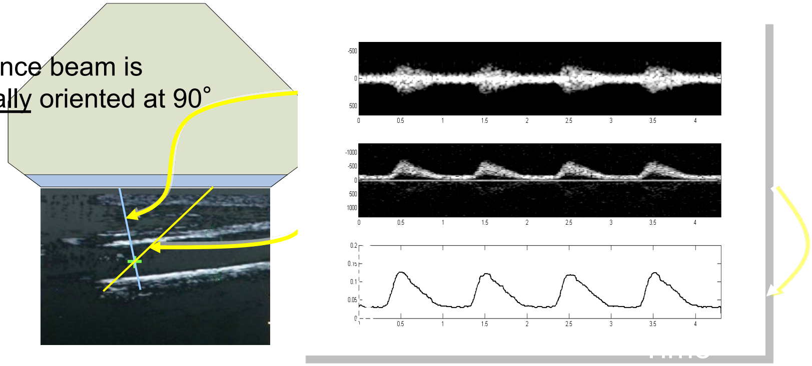


Corresponding spectrum is symmetrical around zero frequency

Slide courtesy of Piero Tortoli, University of Florence

Automatic transverse angle tracking

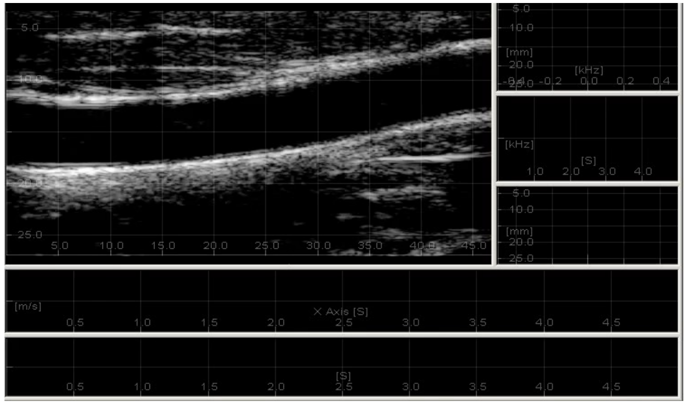
The reference beam is <u>automatically</u> oriented at 90° to the flow

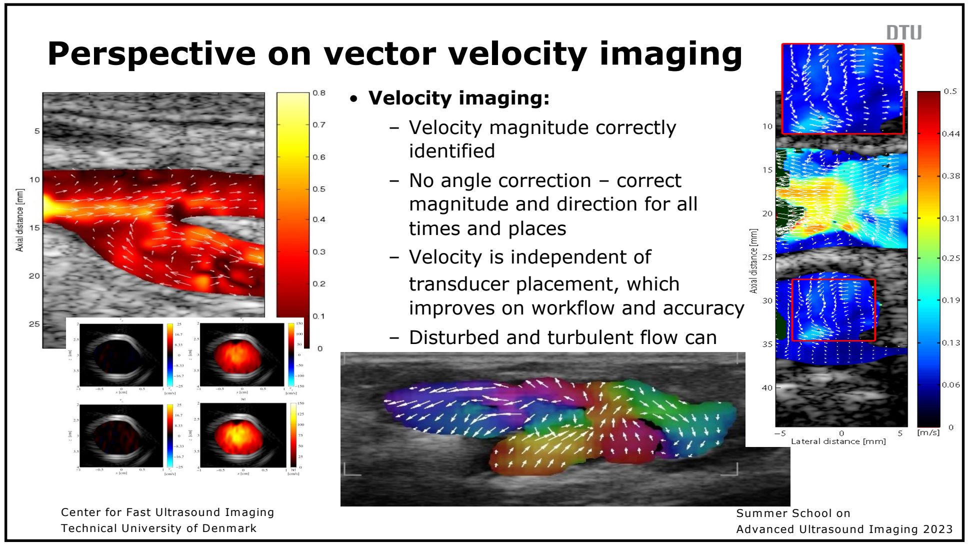


Slide courtesy of Piero Tortoli, University of Florence

In vivo Test

Slide courtesy of Piero Tortoli, University of Florence





Perspective on vector velocity imaging

- **Velocity imaging:**
  - Velocity magnitude correctly identified
  - No angle correction – correct magnitude and direction for all times and places
  - Velocity is independent of transducer placement, which improves on workflow and accuracy
  - Disturbed and turbulent flow can